

PHARMACOLOGICAL CONTROL OF THE CEREBRAL CIRCULATION*

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PHYSIOLOGICAL CONCEPTS

This review is about control of a physiological variable; what that variable's function is and how it is regulated must be discussed first to establish a rational basis for its control. The reader is referred to some excellent recent reviews on regulation of cerebral blood flow (CBF)¹ (1-3). We emphasize here some functions of CBF that are not so obvious and have been largely overlooked.

Cerebral blood vessels evolved as the volume of neural structures made diffusion an inefficient process to supply oxygen and nutrients to nerve cells. This being the primary drive, a close correlation can be found between intercapillary distance or capillary surface area and the level of energy exchange of the various brain regions (4-6). This structurally determined

¹Abbreviations used: acetyl-coenzyme A, Acetyl-CoA; acetylcholine, ACh; adenosine triphosphate, ATP; central nervous system, CNS; cerebral blood flow, CBF; cerebral glucose utilization, CGU; choline, Ch; choline acetyl-transferase, ChAT; chronic obstructive pulmonary disease, COPD; endothelium derived relaxing factor, EDRF; gamma-amino butyric acid, GABA; glutamic-acid-decarboxylase, GAD; magnesium sulfate, MgSO₄; partial pressure of CO₂, PCO₂; positron emission tomography, PET; serotonin, 5-HT; single photon emission computed tomography, SPECT.

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coupling between neural function and blood flow takes care of the anatomical diversity of the nervous system that imposes extremely variable levels of metabolic requirements. This coupling between blood flow and function is determined during development and remains essentially stable throughout adult life.

On the other hand, adaptation to a dynamic environment imposes varying functional regimes for the whole brain or parts of it. As far as the brain as an ensemble is concerned, we can cite the blood flow adjustments that occur through the sleep-wakefulness cycle (7, 8) and the mental activity-relaxation cycles (9). Temporary shortages of the supply of energy substrates such as during hypoxia also require transient global adjustments of the cerebral circulation (2). Very localized changes on the other hand can be induced by sensory stimulation (10–12). These adjustments require rapid variations in cerebrovascular resistance to make possible a greater rate of local cerebral perfusion to increase the delivery rate of energy substrates. But there are other consequences of an increased tissue circulatory convection. The level of tissue CO_2 , for instance, is reciprocally related to the rate of CBF if the production of this metabolite is constant (13). It is well known that PCO_2 is a determinant of neural reflex excitability (14–16). Variations in the rate of blood flow, if induced in the absence of changes in CO_2 production, may therefore be paralleled by proportional changes in reflex function.

Blood flow can also influence synaptic transmission in a more direct way. After a neurotransmitter has been released, it is subjected to a process of elimination from synaptic sites by three main mechanisms: enzymatic degradation, re-uptake into synaptic terminals, and diffusion. The last is facilitated by circulatory convection since the capillaries act as sinks, maintaining a steep gradient that makes the diffusion mechanism efficient. An active synaptic center needs a rate of blood flow in phase with its level of activation to work under optimal conditions, not only to provide adequate energy supply but also to assist in termination of transmitter action. Classic proof of this phenomenon was given by the ganglion perfusion experiments of Feldberg & Gaddum (17) and MacIntosh (18) in which acetylcholine (ACh) was recovered from the venous effluent in amounts commensurate with the level of synaptic activity. This is a pertinent example since diffusion is the main mechanism of termination of ACh action in sympathetic ganglia.

Regulation of acetylcholine synthesis within the central nervous system includes an important role for the vascular system, schematically depicted in Figure 1. ACh is synthesized in the brain from choline (Ch) and acetyl-coenzyme A (Acetyl-CoA) by a reversible reaction catalyzed by choline acetyl-transferase (ChAT) (Figure 1, no 1). The rate of synthesis of ACh appears to be regulated by the availability of the precursors and concentration

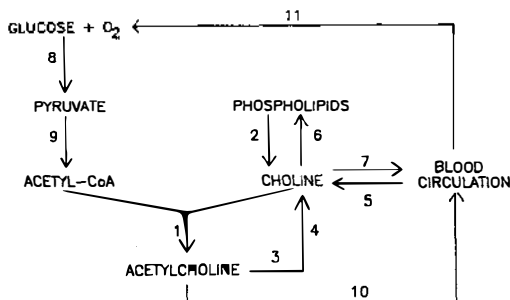


Figure 1 Interactions between ACh synthesis and CBF. Numbers in this scheme correspond to those within parentheses in the text description.

of the products (19–21). Since methylation of phosphatidylethanolamine in brain tissue is very small (20, 22–24), *de novo* synthesis of Ch can be considered negligible. The sources of Ch for ACh formation are degradation of choline-containing phospholipids within the brain itself (Figure 1, no 2), Ch derived from enzymatic hydrolysis of released ACh at synaptic sites (Figure 1, no 3) and salvaged by a high-affinity uptake system (Figure 1, no 4) (19–21), and plasma Ch (Figure 1, no 5). There is a net production of Ch in the brain from phospholipids (Figure 1, no 7) that is removed by the circulation and produces a standing arteriovenous concentration difference (25, 26). Cerebral venous blood contains about 1.5 times higher concentration of Ch than arterial blood entering the brain (27). Given a constant production rate of Ch, it can be hypothesized that the brain concentration of free Ch will bear an inverse relationship to the rate of CBF. In fact, a linear correlation between tissue free Ch and the reciprocal of local blood flow has been found by measuring Ch concentration and local blood flow in the same brain regions of animals with a middle cerebral artery occlusion (28). Since the rate of ACh synthesis is controlled by Ch availability (21, 23), variations in CBF could induce reciprocal changes in the rate of ACh synthesis through this mechanism.

The other precursor of ACh, acetyl-CoA, is generated by oxidative decarboxylation of pyruvate (Figure 1, no 9) that in turn originates from aerobic degradation of glucose (Figure 1, no 8) (29). This is also a blood flow-dependent process but here the sign is reversed: decreases in blood flow will lead to a decrease of Acetyl-CoA availability and thus slow down the rate of ACh synthesis. Cholinergic function can then be driven in quite opposite ways by changes in CBF. These two sets of processes with opposing influences on brain tissue ACh may balance at CBF levels close to normal, exerting a stabilizing influence on tissue ACh contents. This mechanism

seems to operate even at moderate levels of ischemia, with the result that brain tissue ACh content remains constant in this condition (28). Since the synthesis of ACh obeys the law of mass action (19–21) the excess Ch induced by hypoperfusion compensates for the decrease in acetyl-CoA, the supply of which, as stated above, depends on oxidative metabolism. CBF serves in this case (by virtue of a decreased clearance of Ch) as a means of achieving an “autoregulation” of ACh levels. At a critical level of CBF of approximately 0.02 ml/g/min, however, the limit of operation of this autoregulatory mechanism is reached and tissue ACh concentration falls (28, 30, 31). It is now well established that endogenous ACh can increase CBF (Figure 1, no 10; see detailed discussion below) and we can then envision another feed-back loop that will act to stabilize this variable. A decrease in CBF will increase Ch concentration and by a precursor loading effect enhance availability of ACh, which will, in turn, restore CBF levels.

During the reperfusion following cerebral ischemia on the other hand, oxidative metabolism is restored faster than Ch can be washed out and a condition of high tissue Ch levels is found that leads to a transient excess of tissue ACh, likely brought about by a precursor loading effect (31). In the examples discussed above, the level of blood flow controls the rate of transmitter synthesis, by changing the availability of its precursors.

An analogous phenomenon may operate regarding the synthesis of gamma-amino butyric acid (GABA). The enzyme that synthesizes this transmitter, glutamic-acid-decarboxylase (GAD), like ChAT, does not depend on oxidative metabolism. Degradation of GABA, however, does (32). It is conceivable that this process may underlie the large increase in GABA tissue levels observed in areas of focal cerebral ischemia (33).

CEREBRAL BLOOD FLOW AS A CONTROLLING VARIABLE

In light of the concepts outlined above, we can then visualize two processes. In one, which for the purpose of this discourse we can call the regulator mode, the flow diagram is: {neural function} → {energy demand} → {CBF} → {energy supply}. The role of CBF in this case is that of a regulatory variable, providing enhanced delivery rates of energy substrates to support function. In the other process, the information flow is: {CBF} → {neuronal environment} → {neural function}. Here, CBF operates to determine the functional level of a neural center through a number of mechanisms such as removal of neurotransmitters after their release, changes in the gaseous and ionic environment, and control of precursor availability for transmitter synthesis.

The first process, in which CBF acts as a regulator, is expressed by the rapid adjustments of CBF levels to metabolic requirements that occur during phasic changes in brain activity. Although the mechanisms that mediate this dynamic coupling are outside the scope of this review, simplistic explanations, such as that of pH as the universal mediator for this phenomenon, have been abandoned (1). There is probably not a single mechanism for this "coupling", given that the degree of matching between CBF and metabolic expenditure varies for different brain regions and that this phenomenon is sensitive to pharmacological intervention in some regions but not in others. For example, the increase in cerebral cortical blood flow that accompanies arousal can be enhanced by inhibition of acetylcholinesterase and blocked by atropine (34, 35). Changes in the slope of the function that relates CBF to cerebral glucose utilization (CGU) for a large number of brain regions have been described following acidosis (36), or administration of indomethacin (37), hydroxybutyrate (38), ergot alkaloids (39), or norepinephrine (40).

The second process mentioned above, in which CBF acts as a controller, requires primary changes in blood flow. This can occur by hemodynamic conditions, such as variations of systemic perfusion pressure outside the limits of autoregulation, or by vascular narrowing or embolism. There are other more interesting possibilities. Changes in cerebrovascular resistance can be induced experimentally by stimulation of discrete regions within the central nervous system (CNS). Both vasodilatation and vasoconstriction have been described (41–44). Both types of responses can be modulated pharmacologically and specific mediators have been proposed for several of these actions. It is then conceivable that certain regions of the CNS might exert their influence over remote ones through blood flow operating in a controller mode, i.e. by acting in anticipation or even in the absence of metabolic variations to induce global changes in neuronal excitability. Although the concept exposed above is still largely hypothetical from the physiological point of view, it is clear that pharmacological intervention can induce primary vascular effects with functional consequences.

THE CHALLENGE OF A COMPLEX SYSTEM

Cerebral resistance vessels are unique in that they are embedded in a neural matrix. In any other organ, neural effects can be ruled out by selective neurectomies. For example, the role of autonomic and dorsal root afferents have been dissected in many organs with great accuracy and detail by selective ablations. No such accurate dissection is possible in the CNS except by the use of neurotoxins, or by electrical stimulation in a volume conductor, both of which offer little selectivity. Furthermore, the brain is the most

heterogenous of all organs and is so structured that unitary analysis is only possible with great limitations.

Measurement of force development by isolated cerebral vessels *in vitro* is being used increasingly to analyze this element of the complex system, but the results in this situation may have little resemblance to the *in vivo* ones. Sokoloff referred thus to cerebral metabolism: "The *in vitro* techniques establish only the existence and potential capacity of the enzyme systems required for the utilization of a given substrate; they do not define the extent to which such a pathway is actually utilized *in vivo*" (45). This concept can be extended to the cerebral circulation. Receptors present in cerebral vessels are hidden *in vivo* to most substances, from the blood side by the blood-brain barrier in the endothelium and from the tissue side by a tight covering of glial end feet. These barriers disappear in *in vitro* preparations that, in addition, are limited to the study of relatively large conducting vessels. Thus, paraphrasing Sokoloff, we can say that such techniques reveal the existence of potential vasoactive mechanisms, only a subset of which may represent the physiological mechanisms. Likewise, pharmacological effects demonstrated *in vitro* cannot be extrapolated to the *in vivo* situation.

A clear example can be found in the effects of physostigmine on CBF shown in Figure 2. *In vitro* techniques tell us that vasodilatation in response to ACh is an endothelium-dependent response that can be found in practically all vessels, including extracerebral ones (46). Moreover, a cholinergic innervation has been demonstrated in extra- and intraparenchymal cerebral vessels throughout the CNS (47, 48) and cholinergic vascular receptors are also widely distributed in the brain (48). All these facts predict a generalized vasodilator effect when the availability of acetylcholine is enhanced through inhibition of the enzyme acetylcholinesterase. However, the result of such intervention in the intact, conscious rat is a very specific increase in CBF in the neocortex, with lack of effect in striatum and olfactory cortex (Figure 2; 49). Other examples can be found in the effects of norepinephrine and serotonin (consistent vasoconstriction *in vitro* and extremely variable effects on CBF) (50), and of indomethacin, which can decrease CBF although no good model of this phenomenon has been described *in vitro* (51). These apparent contradictions stress the limitations of reductionistic approaches that, while necessary to analyze the functional elements, tell little about the response of the intact system which is the ultimate objective of therapeutic efforts.

THE IMPACT OF METHODOLOGICAL INNOVATION

Our concepts of CBF function and control have evolved in parallel with the development of CBF measurement methodologies. Before this variable was

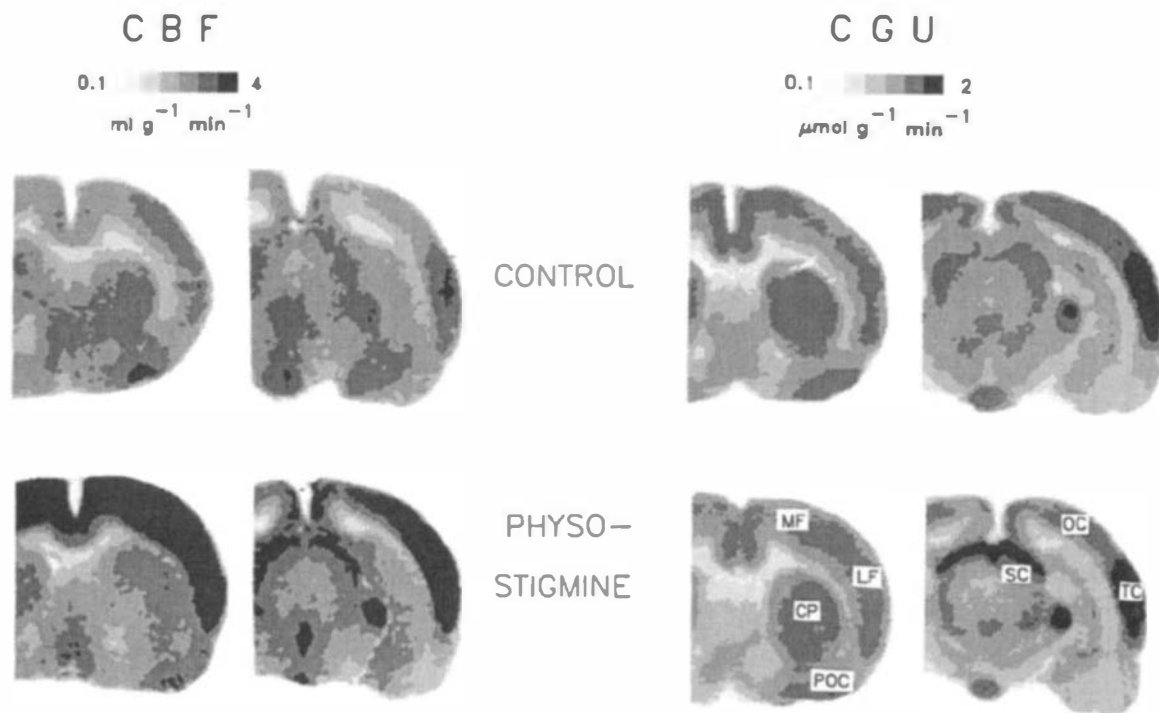


Figure 2 Regional CBF and CGU were measured with iodo- ^{14}C -antipyrine and ^{14}C -2-deoxy-glucose respectively. The figure depicts rat brain autoradiographs at two coronal planes after transformation of optical density to CBF or CGU levels, represented in the corresponding bars. Abbreviations for key structures shown in the right bottom panels are: MF = medial frontal cortex; LF = lateral frontal cortex; CP = caudate-putamen; POC = primary olfactory cortex; OC = occipital cortex; TC = temporal cortex; SC = superior colliculus. Following physostigmine, a marked increase in CBF is observed in frontal, occipital and temporal cortex but without changes in CGU. Superior colliculus shows a parallel increase in CBF and CGU while no changes in CBF or CGU are observed in the rest of the regions. This illustration exemplifies the need for high spatial resolution to reveal regional variations of drug effects on CBF and metabolism.

ever measured, dogma (expressed in the Monro-Kellie doctrine) had it that CBF was invariant. The development of the heat clearance techniques and other measuring devices quickly changed these concepts (52). Not until Kety & Schmidt made (53) the first quantitative measurements of human subjects blood flow, however, were other erroneous theories relating to a determinant role of CBF mental disorders dispelled (54).

The advent of autoradiographic techniques has allowed detection of regional CBF in experimental animals with a spatial accuracy of 10 lines/mm. Since blood flow has practical meaning only in the context of a minimal mass of tissue, certainly greater than a few cells or a single blood vessel, this probably represents the highest resolution worth achieving. In human subjects, positron (55, 56), single photon emission (57), and Xenon-enhanced transmission (58, 59) tomographic procedures have increased accuracy and resolution of CBF measurements over previous bidimensional techniques. This has opened new vistas in pharmacological control of blood flow since this variable can now be explored in very circumscribed areas of the CNS. In keeping with the anatomical and functional diversity of the CNS, wide regional variations in CBF responses to drugs and interventions are now known to occur.

A number of autoradiographic techniques have been designed to obtain pictorial representations of various blood flow-related variables such as glucose utilization (63), tissue pH (61), and protein synthesis (62). The most important of these, in terms of the considerable insight that it has allowed into brain metabolism, is the 2-deoxyglucose methodology developed by Sokoloff and his collaborators (63). An example of the type of information that can be obtained with these techniques is given in Figure 2. Quantitative autoradiography of radioactively labeled compounds permits, in association with CBF autoradiography, a very accurate determination of drug concentration-CBF relationships (64).

All blood flow imaging techniques are based on exchange of a tracer molecule between blood and tissue. This imposes time limitations so that the blood flow measurements obtained in this way represent an average over a period of time in the order of minutes. Rapid adjustments of CBF are then not detected. A number of techniques are available in experimental animals to follow rapid changes in CBF. Most rely on electromagnetic or doppler ultrasound measurements on large vessels supplying or draining brain regions with minimal or no extracerebral contamination. This has been possible in baboons (65) and rabbits (66). These animals possess internal carotid arteries that irrigate almost exclusively the forebrain, whereas other animals require intricate dissections and multiple blood vessel occlusions to isolate the cerebral circulation. In human subjects, the introduction of the duplex doppler ultrasound technique allows a similar time resolution to be achieved by noninvasive measurements of blood flow of the internal carotid artery ex-

tracranially (67) or of intracranial blood vessels (68). These techniques are particularly useful to assess cerebrovascular adaptations in which the time factor is of critical importance, as in the adjustment of cerebrovascular resistance to changes in arterial blood pressure (69). Transcranial doppler ultrasonography has provided information on the dynamic response of regional CBF to sensory activation. A recent elegant study by Conrad & Klingelhöfer (68) has described the dynamic effects of complex visual patterns on local perfusion of the occipital cortex of human subjects and this provides complementary information to that of PET imaging studies (11). Unfortunately, neither in animal experimentation nor in human studies can a single CBF-measuring technique achieve both adequate spatial and temporal resolution.

The tissue hydrogen clearance, first used in the brain by Misrahy & Clark (70), has provided useful insights into the relationships between local blood flow and somatosensory-evoked potentials in experimental animals. This technique is based on the Fick principle. Typically, hydrogen gas is administered by inhalation at a small (3%) nonflammable concentration. A platinum electrode is inserted in the desired region to detect tissue hydrogen concentration amperometrically. When hydrogen gas administration is interrupted, its concentration in tissue decays following first order kinetics. The coefficient of the logistic washout slope represents tissue blood flow (71). The electrodes must be made of small dimensions (typically 25 μm) to avoid tissue injury and artifactual modification of blood flow. Electrode voltage can be recorded in parallel to hydrogen current to analyze electroencephalographic or evoked activity from very small regions within the CNS (34). In this way, Branston et al (72) have correlated somatosensory-evoked activity with blood flow following middle cerebral artery occlusion, and determined the blood flow thresholds for abolition of the different components of this response. It is interesting that certain pharmacological effects on the cerebral cortex, such as the cholinergic inhibition of somatosensory-evoked activity, do not have a metabolic correlate, i.e. are not amenable to analysis by measurement of CGU. We used the H_2 clearance technique to study this phenomenon and thus discovered a dissociation between electrical activity and blood flow under the action of direct cholinergic agonists that induced a substantial increase in local cortical blood flow at a time when the somatosensory response was maximally inhibited (34).

INTRACEREBRAL STEAL, A MYTH?

Focal cerebral ischemia is a situation in which increasing CBF seems an obvious therapeutic option. Two questions must be answered, however, before that task is even attempted: (a) can cerebral vasodilators improve blood

flow in ischemic areas? and (b) if so, can any benefits be expected from such intervention? There is a long history behind the first question. It was widely held during the first three quarters of this century that CBF was regulated by local pH and that areas of cerebral ischemia were acidotic and maximally dilated. It was believed that the use of cerebral vasodilators under such circumstances could only decrease CBF in ischemic areas that could not dilate further, by diverting it to normally perfused tissue that could (intracerebral steal). The theoretical foundation of this concept rests on the assumption that normal and ischemic tissues constitute two hydraulic resistances in parallel supplied by the same vessel and that neither the parent vessel nor the ischemic tissue arm of the network can decrease its resistance in response to the dilator action.

These two assumptions have been challenged by direct measurements of such resistances in cats. Vasodilator drugs were found to decrease consistently the resistance of the vessels supplying the ischemic tissue and in many cases the vascular resistance of the ischemic tissue itself (73). In spite of early experimental evidence for the existence of intracerebral steal (74–76), there are numerous circumstances in which no intracerebral steal, but rather an increase in blood flow of ischemic areas has been found with the use of cerebral vasodilators such as CO₂ (77, 78), papaverine (79), nimodipine (80), and physostigmine (81) in experimental animals. More evidence against the intracerebral steal concept is provided by studies with acetazolamide, a carbonic anhydrase inhibitor. This agent induces cerebral vasodilatation in normal and ischemic brain (82) by a mechanism that is still poorly understood. The simplicity of its use and the rapid and transient nature of its effect has made this substance a useful tool to explore cerebrovascular responses in humans. Single photon emission computed tomography (SPECT) measurements have shown that CBF increases more in normal than in ischemic regions, enhancing contrast between these areas and facilitating diagnosis. In all cases of a series reported by Chollet et al (83), cerebral vasodilatation in response to acetazolamide was depressed in the symptomatic hemisphere in comparison to the asymptomatic one but no instances of a decrease in CBF in the symptomatic side were observed.

The second question posed above has to be approached with knowledge of the physiological response to cerebral ischemia. When blood flow through one of the main cerebral vessels is interrupted, a gradient of ischemia is observed. A central area of minimal blood flow that may lead to permanent tissue damage is surrounded by a zone of subnormal blood flow. Although electrical activity may be suppressed in this zone, commonly referred to as the “ischemic penumbra” (84), ion homeostasis and cellular structure are minimally altered. Strong et al (85) found the levels of CBF in this area to be comparable to those compatible with total restoration of function upon

reestablishment of normal perfusion. This zone of "penumbra", which has been recently detected in cases of human stroke (86–88), may eventually recover full neural function if its vascular resistance can be lowered so as to restore normal blood flow. Trials in human subjects, with measurement of CBF with SPECT techniques, have already shown the possibility of increasing blood flow in this area with hemodilution (89), nimodipine (90), and physostigmine (91). Functional status following these interventions has so far been studied only in the case of hemodilution in which a definite improvement, related to the magnitude of the CBF changes, was found (89, 92). Beneficial effects of nimodipine in ischemic stroke have also been reported (93) although effects of this drug on intracellular calcium may be in part responsible for this outcome.

STRATEGIES TO ENHANCE CBF

Several strategies have been tried to accomplish this task. These can be grouped according to the basic physiological principles involved: Increase in perfusion pressure, decrease in cerebrovascular resistance, and decrease in blood viscosity.

Changes in perfusion pressure When the deficit in cerebral perfusion is the consequence of hemodynamic failure, drugs used to restore peripheral vascular tone should not affect cerebral vascular resistance or metabolism. Both phenylephrine and epinephrine seem to fulfill such requirements (94). Aggressive pharmacological lowering of blood pressure in patients with malignant hypertension may induce cerebral ischemia at blood pressure levels that would be considered satisfactory in normal subjects (95). This is probably due to a reduced autoregulatory capacity of the cerebral circulation in chronic hypertension (96, 97) and highlights the need for careful evaluation of cerebrovascular physiology in these patients before attempting such therapy and for gradual lowering of blood pressure while monitoring brain function.

Cerebrovascular resistance It is not possible to offer a rational classification of drugs capable of inducing a decrease in cerebrovascular resistance. Very few of these drugs show specificity for the cerebrovascular bed and practically none of them are devoid of nonvascular effects on neural function. The effects of drugs on the cerebral circulation need to be analyzed in parallel with an indication of their effect on cerebral metabolism and peripheral vascular resistance. Given the abundance of natural substances with vasomotor activity within the CNS, the possibility of indirect effects of vasodilators, via release of endogenous amines or peptides, has to be considered in every case. The

same applies to the effects of anesthetics and changes in blood gas composition when it comes to their effects on cerebrovascular resistance.

Adrenergic effects on the cerebral circulation have been extensively studied (50). Enhancement of CBF with adrenergic agonists can only occur through increase of arterial blood pressure when the higher limit of autoregulation is exceeded or in cases of hypotensive shock when blood pressure is raised from levels below the lower limit of autoregulation (94). In conditions of preserved autoregulation, either no effect or a small decrease in CBF is found (50, 94, 98). The absence or small magnitude of the cerebral vasoconstriction observed with adrenergic agents is commonly attributed to restrictions in brain tissue access of the drugs imposed by the blood-brain barrier (99). This may not be the complete explanation, however, because topical application of norepinephrine to the cerebral cortex, bypassing the blood-brain barrier, does not induce changes in cortical blood flow either (100); moreover, infusion of norepinephrine directly into the hypothalamus (101) or intraventricularly (102) enhances rather than decreases CBF. These observations contrast with *in vitro* experimentation in which isolated cerebral vessels contract in response to norepinephrine (103). The differences between *in vitro* and *in vivo* approaches probably do not have a simple explanation and may be related to indirect vasodilatation induced by metabolic effects (102) or the release of vasodilator substances.

The vasodilator effects of ACh and other Ch esters on the cerebral circulation, documented by observation of pial vessels, brain temperature, brain volume changes, and blood flow in the carotid artery, have been known since 1929 and have been reviewed by Sokoloff (104). In 1973, using the H_2 clearance technique, a quantitative assessment of this phenomenon was obtained in the cerebral cortex of the rat (34). ACh in the presence of physostigmine, carbachol, arecoline, or pilocarpine, applied topically to the exposed cortex to circumvent the blood-brain barrier, markedly increased local CBF (34). The increase in CBF observed during arousal was tested to ascertain whether it could be mediated by ACh, known to be released in this condition (105). The results showed that in the presence of locally applied physostigmine, the increase in local CBF associated with cortical arousal reached 250% of control, as opposed to 150% observed in the absence of this drug. Conversely, in the presence of locally applied atropine, the hyperemia of cortical arousal was completely blocked. This was the first indication of a physiological role of endogenous ACh in the control of cortical blood flow.

There were other possible explanations for these results, however, such as the possible involvement of changes in cortical metabolism in the presence of these drugs. Cholinergic agonists could have increased neuronal metabolic rate, affecting blood flow through release of vasoactive metabolites. To test this possibility, GABA or $MgSO_4$ was applied to the cortex to abolish

neuronal discharges completely, as evidenced by microelectrode recordings. After this was accomplished, cholinergic agonists were still able to enhance local CBF, a fact interpreted as disproving a neuronal mediation of these effects. Years later, we were able to measure the oxygen consumption of the cerebral cortex in rabbits (106) and the brain regional glucose utilization in rats (49) during the vasodilatation elicited by physostigmine and found that none of these variables was affected during this phenomenon.

It is now clear that cholinergic agonists increase CBF by a primary vascular action and that endogenous ACh may play a significant role, still to be elucidated in detail, in cortical vascular physiology. Considerable evidence has accumulated to favor these ideas. The pioneer findings of Molnár et al (41), Shalit et al (107), and Meyer et al (42) implicating central neural mechanisms in the control of CBF have been followed by numerous similar observations (43, 44, 108–110). The early work of Edvinsson et al (111) pointing to a cholinergic innervation of cerebral vessels has also been amply confirmed over the years with more specific techniques (47) and biochemical probes (112–114). The dilator effect of ACh on cerebral blood vessels *in vitro* (50) is now known to be mediated by an endothelium derived relaxing factor (EDRF) (115). Identity of EDRF with nitric oxide is supported by a large body of work, recently reviewed by Ignarro (116). As discussed above, the role of EDRF in the cerebral vasculature *in vivo* is still unclear.

Although there is no doubt that endogenous ACh can induce significant changes in CBF, the sites from which this mediator is released to induce its effects are still a matter of controversy. The cranial parasympathetic nerves have been explored extensively with variable results. Either no changes in CBF (42, 117–119) or increases smaller than those seen with physostigmine (120–122) have been reported following electrical stimulation of these nerves. Since cortical arousal, as discussed above, can also induce an atropine-sensitive vasodilatation, the spreading of stimulating current to afferent nerves with secondary arousal can provoke misleading results (119). Very few studies have controlled for this source of artifact by electrical recording or measurements of metabolic variables and this may explain the extreme variability of the results of stimulation of parasympathetic nerves on CBF. The simple expedient of ablating these nerves should abolish the vasodilator effect of cholinesterase inhibition with physostigmine that depends on endogenous ACh. The results of such experiments have been negative, however (119).

The role of an intrinsic cerebral system in cholinergic vasodilatation is suggested by the fact that this phenomenon can be elicited by stimulation of the brain stem (43) or cerebellum (110). Iadecola et al have reported that a lesion in the nucleus basalis can block such effects (123). Recently, a very careful study by Lacombe et al (109) has provided evidence that stimulation of the nucleus basalis of Meynert can increase cortical blood flow and that the

effect is blocked by scopolamine. Similar results were reported by Biesold et al (124). If the nucleus basalis is the sole source of cholinergic cortical nerve fibers that innervate cerebral blood vessels, destruction of this nucleus should prevent the vasodilatation induced by cholinesterase inhibition. This has been recently shown in our laboratory not to be the case (125). Ibotenic acid lesions of this structure did not impede the cortical vasodilatation induced by physostigmine. This result implies that the source of cortical cholinergic vascular afferents is not in the nucleus basalis and stimulation experiments may have activated cortical afferents capable of triggering arousal with the concomitant cholinergic vasodilatation. Alternatively, redundant cholinergic fibers could have reinnervated the cortical vessels in the period between the nucleus basalis lesion and the blood flow experiment (10 days). Further experimentation will be required to explore these possibilities. Alternative potential sources for the endogenous ACh that mediates the regulatory functions described above are other basal forebrain regions, the ponto-mesencephalic tegmentum (126) and intrinsic cortical neurons of the cortex (127); these are worth exploring experimentally.

Serotonin (5-HT) reliably contracts cerebral blood vessels *in vitro* (128) but it does not cross the blood-brain barrier (129). Although there is no clear indication for a physiological role of 5-HT in CBF regulation, intravenously administered ketanserin, a 5-HT antagonist, has been shown to block remote decreases in CBF associated with cerebral embolization (130), suggesting a role of endogenously released 5-HT in this phenomenon. It has been known for a long time that 5-HT is released in areas of ischemia (131) and these facts may rekindle the interest in therapeutic applications of 5-HT blockers in this condition.

The effects of adenosine on the cerebral circulation and its involvement in CBF regulation have been recently reviewed by Phillis (132). This metabolite induces cerebral vasodilatation upon intravenous administration but it is not very specific since peripheral vasodilatation with a drop of blood pressure also occurs. The effect on CBF is strong enough, however, to induce significant vasodilatation in humans (133). The cerebral vasodilator effect of ATP seems to surpass that of adenosine (134), however, and the Cobalt-ATP salt, with a longer half-life, offers promise as a therapeutic agent (135).

Prostaglandins are synthesized by cerebral blood vessels (136). Numerous observations, reviewed by Walker & Pickard (51), suggest a role of eicosanoids in cerebrovascular regulation. Prostacyclin has been characterized as a cerebral vasodilator both *in vitro* and *in vivo* (136) but therapeutic trials in patients with acute cerebral infarction have failed to demonstrate any effects on CBF or neurological status (137). Indomethacin has been reported to attenuate the CBF increase induced by hypercapnia, a phenomenon that seems

to be species-specific (51). A remarkable decrease in CBF, with no apparent ill effects, is known to occur in infants given this drug for the purpose of closing the ductus arteriosus (138–140).

Calcium channel blockers have been extensively studied as cerebral vasodilators of potential use in cerebral ischemia. The better known drug of this group regarding these effects is nimodipine, a 1,4-dihydropyridine. This agent decreases cerebrovascular resistance more than peripheral vascular resistance and effects an increase in CBF at low doses. Dose escalation induces a decrease in arterial blood pressure that offsets the benefits of decreased cerebrovascular resistance (141). No cerebral metabolic changes are induced by nimodipine in intact brains (142, 143) but the normalization of oxidative metabolism after transient ischemia is accelerated (143). Studies in human subjects have shown improvement of CBF in the area of penumbra in stroke patients (90). Beneficial effects of this drug in experimental models of cerebral ischemia remain controversial (144) but clinical trials have been encouraging (93).

UNDESIRABLE DRUG EFFECTS ON CBF

Often drugs given for other therapeutic reasons have a significant effect on CBF, creating a potential for complications in patients at risk. For instance, anticholinergics impair CBF regulatory functions in experimental animals (34) and scopolamine decreases CBF in the cerebral cortex of humans (145). It is then conceivable that drugs with anticholinergic effects commonly used for the treatment of depression may be detrimental to CBF regulation.

The same can be said of nonsteroidal anti-inflammatory drugs. Indomethacin blocks several important CBF regulatory mechanisms in animals and humans (51) and it seems that the use of these agents in patients with cerebrovascular insufficiency should be re-examined. Recently, cimetidine has been reported to block the cerebrovascular vasodilatation in response to hypoxia (146), one of the basic CBF regulatory mechanisms, implying a role of histamine in this response. The use of these drugs should be considered with caution in patients at risk for hypoxic episodes, such as chronic obstructive pulmonary disease (COPD) and sleep apnea.

Aminophylline, a soluble theophylline salt commonly used for patients with COPD, has long been known to decrease CBF in humans (147) and to impair cerebrovascular responses to hypoxia in animals (132). It is surprising that the response of CBF to this drug has been tested only recently in COPD patients. The results have shown significant reductions in CBF at doses customarily used (148) and place a question mark on the use of this drug in COPD patients, particularly in those at risk for cerebrovascular disease.

CONCLUSIONS AND FUTURE DIRECTIONS

CBF should not be viewed merely as a variable that controls the supply of energy substrates and passively follows changes in neuronal metabolism, but rather as a determinant of neuronal function through a number of mechanisms such as removal of released transmitter, control of precursor availability for the synthesis of key molecules, and alteration of composition of the gaseous and ionic environment. All CBF functions mentioned above are amenable to pharmacological control. However, the decision to influence CBF pharmacologically requires knowledge of the particular pathophysiological circumstances and it is there that we lack a solid conceptual framework. Although the last two decades have seen a significant advance in our understanding of the ways in which cerebrovascular resistance is adjusted to meet metabolic demands, the role of CBF in the control of transmitter synthesis and disposal, neuronal electrical functions and regulation of the internal milieu of the brain remains largely unexplored. This configures a vast gap in our knowledge and limits a rational approach to the pharmacological control of CBF. Isolated vessel techniques have been exploited to yield basic information on behavior of cerebrovascular smooth muscle, but the organizational complexities of the nervous system impose limitations to this approach. The ensemble of blood vessels, glial, and neuronal elements possesses properties that cannot be modeled *in vitro*. There is a need for methodological approaches that would maintain nervous structure intact and yet measure CBF with a spatial resolution commensurate with the organizational principles of the brain. The tracer methodologies for measurement of CBF and metabolism pioneered by Kety & Sokoloff have been followed in recent years by techniques that can produce pictorial representations of a large number of blood flow-related variables, as well as of distribution of pharmacological receptors and enzymes. Adequate combinations of these approaches can provide an integral view of the outcome of pharmacological interventions aimed at modifying CBF and of its impact in neuronal metabolism and function. Local application of drugs to selected nervous structures has been used successfully to circumvent complications created by the blood-brain barrier and peripheral drug effects, but coordination of this approach with the tracer techniques mentioned above has not yet been fully exploited. The analysis of pharmacological effects on cerebrovascular regulations has not gone beyond the descriptive phase. We have gathered an impressive inventory of drug effects on contractility of isolated blood vessels, morphology of pial vessels and CBF levels but only sporadic efforts have been devoted to understanding the impact of a varying CBF on neural function.

Interest in the role of CBF in pathophysiology of the nervous system has been rekindled by the recent availability of imaging techniques for CBF and

metabolism that allow studies in human subjects that were previously accessible in experimental animals. It is now clear that CBF can be modified pharmacologically and the outcome monitored with levels of spatial and temporal resolution that were unsuspected before. The limitations are now more in our ideas than in the tools that we possess. The currently prevalent ideas about CBF functions were laid out with brilliant insight by Roy & Sherrington in 1890 (149). They had no other tools at their disposal than a membrane plethysmograph, a lever, and a smoked drum. In the centennial of that event, the challenge is to make intelligent use of the presently available resources to create a new theoretical framework that will advance beyond the ideas of those pioneer scientists.

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